## Non-Gaussian Displacements in Active Transport on a Carpet of Motile Cells

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(Received 25 October 2023; revised 10 January 2024; accepted 24 January 2024; published 23 February 2024)

We study the dynamics of micron-sized particles on a layer of motile cells. This cell carpet acts as an active bath that propels passive tracer particles via direct mechanical contact. The resulting nonequilibrium transport shows a crossover from superdiffusive to normal-diffusive dynamics. The particle displacement distribution is distinctly non-Gaussian even at macroscopic timescales exceeding the measurement time. We obtain the distribution of diffusion coefficients from the experimental data and introduce a model for the displacement distribution that matches the experimentally observed non-Gaussian statistics. We argue why similar transport properties are expected for many composite active matter systems.

DOI: 10.1103/PhysRevLett.132.088301

The collective behavior of active particles is the focus of one of the most dynamically evolving research directions in nonequilibrium statistical and biological physics over the past decade. Active particles [1,2] convert chemical energy into motion and provide a unifying concept for a wide range of systems, such as engineered bipolar "Janus particles" with different sources of activity [3–6], bacterial swimming [7,8] and swarming [9], crawling cells [10], bristle robots (hexbugs) [11–13], or groups of foraging animals [14]. Large ensembles of interacting active particles, in which energy is continuously injected and dissipated locally, operate far from thermodynamic equilibrium. This gives rise to a plethora of nonequilibrium phenomena, such as the emergence of large scale patterns [15], topological order [16], or nonequilibrium phase separations [17–19], and raises questions about the thermodynamics of such systems, e.g., their pressure [20-22]. All these features are studied under the common theme of active matter [23,24].

In many real-world settings, active agents interact with passive objects in their surroundings that introduce additional degrees of complexity ("composite active matter" [25]). For instance, boundaries and obstacles may rectify their motion [26], self-similar structures may emerge at interfaces in active matter invasion [27], or nonisotropic passive objects, such as gears [28,29] or curved tracers [30], can be powered by an "active bath" of self-propelled particles to perform coherent motion. For a fundamental understanding as well as for many applications, the statistics of transport in a bath of active elements is of particular importance. Earlier work has focused on tracer diffusion in active fluids composed of suspensions of biological swimmers, such as bacteria [31,32] or algae [33,34], agitating the surrounding fluid of the bath, or particles in the vicinity of flow-generating active carpets [35]. Nontrivial scalings with several crossovers in the

mean-squared displacement (MSD) of passive tracer particles were observed; for a review, see Ref. [2]. However, little is known about the statistical properties of other types of active baths. A particularly large and important class are composite systems, in which the interactions between active elements and passive tracers are established by direct mechanical contact and adhesion instead of fluid flows and hydrodynamic interactions. This situation arises, for example, when slowly moving, adherent cells interact with passive objects, and it has important practical implications for the movement of foreign bodies in tissues or the delivery of drug-loaded particles in a multicellular environment.

Here we consider such a composite biohybrid system as a paradigmatic showcase of an active bath, in which passive objects are agitated and transported by self-propelled agents via direct mechanical contact. As an active bath, we use a monolayer of cells of the social amoeboid Dictyostelium discoideum, an established model organism with well-characterized properties [36]. As D. discoideum cells show unspecific adhesion to most common material surfaces [37], adhesive contacts between cells and microparticles are formed upon collision and may spontaneously break again [38]. No specific surface functionalization is required. Unbound cells can freely move over the twodimensional substrate. When cells bind to the microparticles, the active motion of cells results in nonthermal fluctuating forces that randomly displace the particles. While this process has been studied in detail for single cells interacting with a single particle [25,39], we here consider particles that are attached to many cells at the same time. We performed time-lapse recordings with a time interval of 15 s between frames over a duration of 4 h. In total, 174 particle trajectories were extracted; the majority were longer than 2.5 h [40]. An example from the recorded

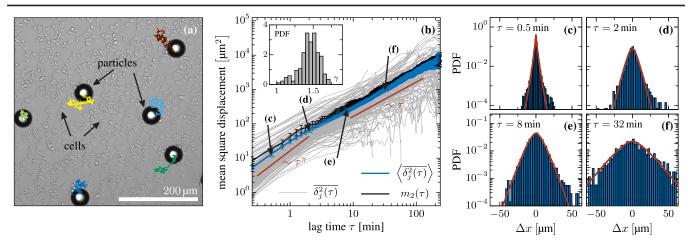


FIG. 1. Characteristics of cargo particle transport on cellular monolayers. (a) Illustration of an experimental bright-field microscopy recording with particle trajectories displayed as colored overlays (see the Supplemental Material [40] for a video). Bright spots with a black halo are particles (46 µm diameter). Cells with an extension of about 10 µm appear translucent in the background. (b) MSD as function of lag time  $\tau$ : TAMSDs  $\overline{\delta_j^2(\tau)}$ , Eq. (1), of individual particles (light gray lines), their ensemble average  $\langle \overline{\delta_j^2(\tau)} \rangle$  (blue), and the ensemble-averaged MSD  $m_2(\tau)$  (black). Error bars indicate 1 $\sigma$ -confidence intervals. These MSDs reveal two distinct regimes: superdiffusion at short timescales ( $\tau \leq 2$  min) and normal diffusion at long times ( $\tau \geq 2$  min). Inset: scaling exponents  $\gamma$  obtained by fitting  $\overline{\delta_j^2(\tau)} \sim \tau^{\gamma}$  to the first three data points of TAMSDs (time interval: 45 s). (c)–(f) The non-Gaussian displacement PDFs along the x axis for different lag times. Red line in (c): stretched exponential distribution, proportional to  $\exp(-a|\Delta x|^{\delta})$  with an exponent  $\delta \approx 0.77$ ; red lines in (d)–(f): predicted displacement distributions, based on heterogeneous Brownian motion. The respective parameters inferred from the distributions shown in Figs. 3(a)–3(c) were used to plot the PDFs in (d)–(f) [for details, see Eqs. (5) and main text].

image stacks is shown in Fig. 1(a), with the particle trajectories displayed as colored overlays (see Material and Methods in the Supplemental Material [40] for experimental details). From the trajectories, we characterized the dynamics of particles on the cell layer in terms of their MSD, their displacement probability density functions (PDFs), and their displacement autocorrelation function (DACF).

MSD crossover from superdiffusive spreading to normal diffusion.—Position time traces  $\mathbf{r}_{j}(t)$  of length T of individual particles (index j) are evaluated in terms of the time-averaged MSD (TAMSD) [43],

$$\overline{\delta_j^2(\tau)} = \frac{1}{T - \tau} \int_0^{T - \tau} |\mathbf{r}_j(t + \tau) - \mathbf{r}_j(t)|^2 dt, \qquad (1)$$

where  $\tau$  is the lag time. The ensemble mean-TAMSD is defined as  $\langle \overline{\delta_j^2}(\tau) \rangle = N^{-1} \sum_{j=1}^N \overline{\delta_j^2}(\tau)$ . From an ensemble of particles, one can also determine the ensemble-averaged MSD  $m_2(\tau) = N^{-1} \sum_{j=1}^N [\mathbf{r}_j(\tau) - \mathbf{r}_j(0)]^2$  [43–45]. The results for MSD and TAMSD are displayed in Fig. 1(b). The TAMSDs (light gray lines) reveal a large amplitude spread, indicating significant differences in the transport of individual particles. Their ensemble average, displayed as the blue line, exhibits two regimes: superdiffusion  $\langle \overline{\delta_j^2(\tau)} \rangle \simeq \tau^{\gamma}$  at short lag times with an anomalous diffusion exponent of approximately  $\gamma \approx 1.45$  (median) and normal diffusion ( $\gamma \approx 1$ ) at long lag times. Before the crossover time  $\tau \approx 2$  min, individual TAMSD scaling exponents vary between  $\gamma \approx 1.33$  and 1.57 (1 $\sigma$  interval); the inset in Fig. 1(b) shows a histogram of the exponents  $\gamma$  obtained from fits to TAMSDs.

A similar superdiffusive scaling was observed for the MSD of single cell trajectories [46–50] and is reflected in the trajectories of cargo particles transported by an individual cell [25]. The crossover time to normal diffusion corresponds to a length scale that is comparable to the average cell size (5–10  $\mu$ m in radius). We thus conclude that the short-time superdiffusive scaling reflects the action of individual cells, while the long-term normal diffusion corresponds to collective particle transport involving many cells. Throughout the Letter, we distinguish these two regimes as "short-" and "long-time" transport regimes.

Non-Gaussian displacement distributions.—The PDFs of the particle displacements  $\Delta \mathbf{r}_j(t, \tau) = \mathbf{r}_j(t + \tau) - \mathbf{r}_j(t)$  are shown in Figs. 1(c)–1(f) for different lag times  $\tau$ . The lag times were chosen from the superdiffusive regime [Fig. 1(c),  $\tau = 0.5$  min], close to the crossover time [Fig. 1(d),  $\tau = 2$  min], and from the diffusive regime [Figs. 1(e) and 1(f) with  $\tau = 8$  and 32 min]. Notably, all displacement PDFs are non-Gaussian, with a positive excess kurtosis implying a leptokurtic PDF with a more pronounced peak at zero and heavier tails as compared to a Gaussian distribution. We quantified the degree of non-Gaussianity via an order parameter: the displacement distributions remain non-Gaussian for all considered lag times (data are provided in the Supplemental Material [40]). At short lag times, the displacement PDF is well approximated by a stretched exponential, proportional to  $\exp(-a|\Delta x|^{\delta})$ with  $\delta \approx 0.77$ . With increasing lag time, the PDF changes to a non-Gaussian shape with exponential tails ( $\delta \approx 1$ ) in the Fickian regime ( $\gamma = 1$ ). Below, we describe this exponential PDF by a heterogeneous Brownian diffusion model. We also invoke tempered fractional Laplace motion as a model for all lag times. Please note that the long-time diffusion coefficient of a freely diffusing *D. discoideum* cell is approximately  $D_c \approx 8 \ \mu m^2 / \min [40,51]$ . Hence, the cellular carpet is not stationary: a freely diffusing cell will travel a distance that is comparable to the diameter of a particle ( $d = 46 \ \mu m$ ) within one hour; the experimental duration is 4 times longer. Thus, there is noticeable mixing of cells within the recording time. Nonetheless, Gaussianity is not restored at these timescales.

DACF indicates Brownian motion.—The autocorrelation function of the displacements  $\Delta \mathbf{r}_j(t, \tau)$  of particle *j* is defined as

$$C_{\tau}^{(j)}(\Delta) = \overline{\Delta \mathbf{r}_{j}(t+\Delta,\tau) \cdot \Delta \mathbf{r}_{j}(t,\tau)}$$
  
=  $\frac{1}{T-\Delta-\tau} \int_{0}^{T-\Delta-\tau} \Delta \mathbf{r}_{j}(t+\Delta,\tau) \cdot \Delta \mathbf{r}_{j}(t,\tau) dt$  (2)

and measures the degree of correlation between a particle displacement  $\Delta \mathbf{r}_i(t,\tau)$  in a time interval  $\tau$  starting at time t and a displacement in an interval of the same length  $\tau$ , beginning at the later time  $t + \Delta$ . For small time shifts  $\Delta$ , the displacements are highly correlated, whereas the correlations decay to zero at longer  $\Delta$ . The value of the DACF at  $\Delta = 0$  is identical to the TAMSD  $\overline{\delta_i^2(\tau)}$ , cf. Eq. (1). We focus on the  $\Delta$  dependence of the normalized DACF  $\tilde{C}_{\tau}^{(j)}(\Delta) = C_{\tau}^{(j)}(\Delta)/C_{\tau}^{(j)}(0)$  as well as on its ensemble mean  $\langle \tilde{C}_{\tau}(\Delta) \rangle = N^{-1} \sum_{j=1}^{N} \tilde{C}_{\tau}^{(j)}(\Delta)$ . The temporal decay of the ensemble-averaged DACF is shown in Fig. 2(a) for different lag times  $\tau$ ; the DACFs of individual particle trajectories, together with their ensemble average, are displayed in the inset for  $\tau = 2$  min as an example. As expected, the degree of correlation increases with  $\tau$ . Notably, the correlations decrease linearly as a function of  $\Delta$  for lag times  $\tau$  in the diffusive regime and are essentially zero for time shifts  $\Delta \geq \tau$ . This is a signature of independent steps in normal Brownian motion, for which the renormalized DACF takes the triangular shape  $\tilde{C}_{\tau}(\Delta) =$  $1 - |\Delta|/\tau$  for  $0 \le |\Delta| \le \tau$  and 0 otherwise [40]. In Fig. 2(b), we show the DACFs as a function of the rescaled time shift  $\Delta/\tau$ . Indeed, the data collapse onto a single master curve for all lag times  $\tau \ge 2$  min, underlining that particle displacements become independent at times of several minutes and beyond.

Fickian yet non-Gaussian particle transport.—Our analysis above reveals that polystyrene spheres on a carpet of cells show distinct characteristics of Brownian motion above the crossover time: the MSD increases linearly and

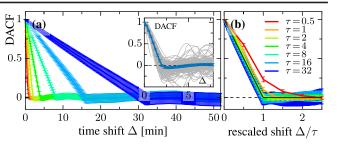


FIG. 2. (a) Ensemble-averaged DACFs for different lag times  $\tau$  as listed in panel (b) (all times in minutes). Gray lines show single-particle DACFs  $\tilde{C}_{\tau}^{(j)}(\Delta)$  for lag time  $\tau = 2 \, \text{min}$  (inset); the ensemble average  $\langle \tilde{C}_{\tau}(\Delta) \rangle$  is depicted in blue—error bars indicate  $3\sigma$ -confidence intervals. (b) The same data as in (a) as function of the rescaled time shift  $\Delta/\tau$ . For lag times  $\tau \geq 2 \, \text{min}$ , the DACF collapses onto a triangular correlation function (black solid line), in line with Brownian motion [40].

the DACF has a triangular shape. However, the displacement PDFs are non-Gaussian. We tested whether the non-Gaussian statistic arises from nonstationary dynamics of the system but did not detect any statistically significant changes in the bead dynamics over time [40].

Non-Gaussian displacement PDFs together with a linear-in-time MSD were observed in different stationary systems, e.g., colloids diffusing along linear tubes, through spatially heterogeneous arrays of pillars [52], or entangled actin networks [53]. Such observations may arise when the diffusion coefficient of a diffusing particle follows a stochastic diffusion process itself ("diffusing diffusivity") [54–58]. If the temporal diffusivity variation is slower than the experimentally relevant timescales, the diffusivity is effectively constant in time but randomly distributed across the diffusing particles [59,60]. We provide evidence from the experimental data in the Supplemental Material [40] suggesting that temporal fluctuations of the diffusivity of individual particles are much weaker as compared to the spread within the ensemble. The PDF of diffusivities across the ensemble introduces an additional level of annealed disorder, also called "superstatistics" [61]. For ensembles of active particles, superstatistical diffusivities and speeds were recently analyzed theoretically [62,63].

Superstatistics of diffusion coefficients.—Long-time particle motion is Fickian, but individual diffusion coefficients  $D_j$  of particles j vary across the ensemble, resulting in the amplitude scatter of individual TAMSDs, cf. Fig. 1(b). We expect that this variability is caused by variations in the size and activity within the population of cells [50]. Moreover, the cell density varies in space due to finite number fluctuations. The spread in  $D_j$  may be enhanced by tugof-war-style competition between individual cells to which the cargo particle is attached. Even though the statistical properties are identical in the long-time limit (independent increments, normal diffusion), quantitative differences in the diffusivities of individual particles are thus expected.

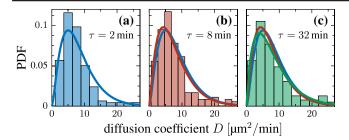


FIG. 3. Histograms of diffusion coefficients for different lag times  $\tau$ . Solid lines represent fits with a gamma distribution [Eq. (3)], inferred by maximum likelihood estimation: (a)  $\alpha = 2.55$ ,  $D_{\beta} = 3.23 \,\mu m^2 / \min$ , (b)  $\alpha = 2.26$ ,  $D_{\beta} = 3.40 \,\mu m^2 / \min$ , and (c)  $\alpha = 1.91$ ,  $D_{\beta} = 4.24 \,\mu m^2 / \min$ . Sample means of diffusion coefficients: (a)  $\langle D \rangle = (8.2 \pm 0.5) \,\mu m^2 / \min$  for  $\tau = 2 \,\min$ , (b)  $\langle D \rangle = (7.7 \pm 0.4) \,\mu m^2 / \min$  for  $\tau = 8 \,\min$ , and (c)  $\langle D \rangle = (8.0 \pm 0.5) \,\mu m^2 / \min$  for  $\tau = 32 \,\min$ . (b) The fit from (a) is shown as an overlay; (c) contains all three fits. Differences are not statistically significant [40].

To test the conjecture that the spread in particle diffusivities may explain the non-Gaussian displacement distributions, we derive the distribution of diffusivities directly from experimental data by estimating the  $D_j$  values of individual cargo particles from their TAMSDs via  $\hat{D}_j = \overline{\delta_j^2(\tau)}/(4\tau)$  for different lag times  $\tau$  (Fig. 3). We quantify the superstatistic of diffusion coefficients by a gamma PDF,

$$P(D) = \frac{1}{\Gamma(\alpha)D_{\beta}} \left(\frac{D}{D_{\beta}}\right)^{\alpha-1} \exp\left(-\frac{D}{D_{\beta}}\right)$$
(3)

with shape parameter  $\alpha$  and scale parameter  $D_{\beta}$ —a widely used heuristic [50,64,65], which provides a reasonable fit to our data and, moreover, enables one to calculate the ensemble-averaged propagator analytically as discussed below [66]. The gamma distributions are consistent over time, i.e., the inferred parameter values are independent of the chosen lag time  $\tau$  and yield a mean diffusion coefficient of  $\langle D \rangle \approx 8 \ \mu m^2 / \min$  in all cases (see caption of Fig. 3 for exact numbers). The consistency is elucidated by the fact that single-particle estimates of diffusion coefficients fluctuate only mildly as a function of the chosen lag time  $\tau$  [40]. This supports our conjecture that long-time active transport of microparticles on a carpet of motile cells is governed by heterogeneous Brownian motion.

Prediction of displacement PDFs.—We verified the consistency of our superstatistical model by comparison of the empirical displacement PDFs to the model prediction. For normal Brownian diffusion, the displacement PDF (given the diffusion coefficient *D*) is Gaussian:  $\rho(\Delta \mathbf{r}, \tau | D) =$  $(4\pi D\tau)^{-1} \exp[-|\Delta \mathbf{r}|^2/(4D\tau)]$ . The displacement PDF of an ensemble of particles with different diffusivities is then obtained by averaging with respect to the distribution of diffusion coefficients *P*(*D*) [59,61],

$$\langle \rho(\Delta \mathbf{r}, \tau) \rangle = \int_0^\infty \rho(\Delta \mathbf{r}, \tau | D) P(D) dD.$$
 (4)

The corresponding displacement PDFs of the *x* and *y* components of  $\Delta \mathbf{r}$  are obtained by marginalization. In the diffusive regime, they were found to be statistically independent (linear correlation coefficient below 0.02 in all cases). We focus on displacements along the *x* axis [67]. Using the gamma distribution model *P*(*D*) to describe the heterogeneity in the diffusion coefficients and the Gaussian propagator  $\rho(\Delta \mathbf{r}, \tau | D)$ , we obtain the displacement PDF

$$\langle \rho(\Delta x,\tau) \rangle = \mathcal{N} \frac{|\Delta x|^{\alpha-1/2}}{(D_{\beta}\tau)^{\alpha/2+1/4}} K_{\alpha-1/2} \left(\frac{|\Delta x|}{(D_{\beta}\tau)^{1/2}}\right)$$
(5a)

$$\simeq \frac{1}{2^{\alpha} \Gamma(\alpha)} \frac{|\Delta x|^{\alpha-1}}{(D_{\beta} \tau)^{\alpha/2}} \exp\left[-\frac{|\Delta x|}{(D_{\beta} \tau)^{1/2}}\right], \quad (5b)$$

where  $\mathcal{N} = 2^{1/2-\alpha}/[\sqrt{\pi}\Gamma(\alpha)]$  is a normalization constant and  $K_{\nu}$  denotes the modified Bessel function of the second kind. Asymptotically, an exponential tail emerges with a power-law correction in  $|\Delta x|$  [Eq. (5b)] that vanishes in the case of exponentially distributed diffusion coefficients  $(\alpha = 1)$  [40]. By derivation, the displacement PDF depends on the similarity variable  $|\Delta x|/\sqrt{\tau}$  only, reflecting the normal-diffusive behavior  $\Delta x^2 \sim \tau$ . The PDF (5a) is compared to experimental data in Figs. 1(d)–1(f). Note that this is not a fit since all parameters in Eqs. (5) were derived from the empirical PDF of diffusion coefficients (Fig. 3). The agreement of the displacement PDFs confirms our hypothesis that individual cargo particles perform Brownian motion with randomly distributed diffusivities.

Discussion.—We found that the nonequilibrium transport of microparticles in an active bath of cells displays a crossover from superdiffusion to Fickian transport with pronounced non-Gaussian displacement PDFs, even in the long-time limit over at least 2 orders of magnitude in time. While the dynamics of each particle becomes Fickian, the diffusivity varies across the ensemble [59]. The active cellular bath constitutes a "heterogeneous diffusion landscape" for particles. We emphasize in this context that the presence of a particle influences the distribution of cells around it, since adherent D. discoideum cells may easily bind to a particle [37,38]. If the cell-particle interactions stabilize the local composition of the cell carpet in the vicinity of a particle, the homogenization of initial fluctuations in the heterogeneous landscape of diffusivities slows down considerably. This may be one of the reasons why a particle is going to explore the entire heterogeneous diffusion landscape on very large timescales only (if it does so at all). Variations of diffusivities may arise from a tug-of-war between multiple cells simultaneously attached to the cargo particle. The tug-of-war may lead to repeated unsuccessful attempts to move the cargo in a given time window. Intermittent motion with distributed immobilization events can be described by subordination of a parent process with a waiting time PDF [68,69]. If the subordinator is a gamma distribution, Brownian motion stays Fickian, yet the displacements follow a Laplace PDF [64,70]. If the parent process is fractional Brownian motion, a Gaussian process with power-law correlated increments [71,72], the subordination by the gamma distribution produces a PDF with stretched tails proportional to  $\exp(-a|\Delta x|^{\delta})$ , the stretching exponent of which is  $\delta = 2/(1 + \gamma)$  [65]. The DACF derived from our experimental data at short times ( $\tau < 2 \text{ min}$ ) indeed shows positive values beyond the rescaled time shift  $\Delta/\tau = 1$ , reminiscent of fractional Brownian motion. Thus, assuming fractional Laplace motion (FLM) for the cargo particle transport dynamics, superdiffusion in the short-time regime with an exponent of  $\gamma \approx 1.45$  (median of the observed exponents, cf. Fig. 1) would imply a stretching exponent of  $\delta \approx 0.82$ , which is close to the experimentally inferred  $\delta \approx$ 0.77 as shown in Fig. 1(c). Assuming that the power-law correlations have a finite cutoff that reflects the observed crossover from super- to Fickian diffusion, the motion at long times ( $\tau > 2$  min) would change from  $m_2(\tau) \simeq \tau^{\gamma}$ to  $\simeq \tau$  [73], and the displacement PDF exhibits exponential tails ( $\delta = 1$ ), in line with our experimental observations. More refined data will be needed to connect the observed motion with potential tug-of-war immobilization events. Furthermore, it will be of interest to discuss asymptotic Laplace displacement PDFs and FLM in a wider context of anomalous diffusion processes in the future [56,69,74,75].

Non-Gaussian statistics due to (dynamic) heterogeneity has already been reported for acetylcholine receptors on live muscle cell membranes [76] and for cytoplasmic mRNA molecules in both E. coli and yeast [77]. Here, we demonstrate that anomalous effects may also arise at the level of interacting cells when collectively moving passive microobjects. Since cell-cell heterogeneity and fluctuationdominated dynamics are ubiquitous in biological systems, our findings are relevant beyond our specific model system, for instance, when microparticles are exposed to migrating neutrophils. Generally, foreign bodies that interact with a dynamic tissue environment are key to many medical applications-oral vaccination strategies [78] or the assimilation of environmental microplastics in the body [79] both rely on the intestinal uptake of microparticles. Options to guide the cell-driven microtransport by chemical gradients [38] make this process particularly attractive for drug delivery applications.

We thank Kirsten Sachse for supporting laboratory routines. This research has been partially funded by Deutsche Forschungsgemeinschaft (DFG), Grants No. 318763901–SFB1294 (R. G., L. B., T. M., and C. B.), No. 116203121–BE 3978/3-3 (S. S. P. and C. B.), and No. ME 1535/12-1 (R. M.).

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